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Review Article

Current methods of focal liver lesion diagnosis



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ABSTRACT

Introduction: The widespread availability of non-invasive radiological and diagnostic imaging techniques significantly contributed to the detectability of focal lesions in the liver. Ultrasonography, computed tomography (CT) multidetector CT (MDCT), conventional magnetic resonance imaging (MRI), diffusion-weighted magnetic resonance imaging (DW-MRI) and isotope imaging are used for focal liver diagnosis.

Aim: This article reviews the available methods for diagnosing focal liver lesions on the basis of current literature.

Discussion: The diagnostic precision of a conventional ultrasound test in detecting and differentiating focal hepatic lesions is estimated at 62%. Its sensitivity for the detection of metastases ranges from 40% to 80%. If the majority of metastatic tumors are small, the sensitivity of ultrasound tests decreases dramatically to 20% for foci smaller than 1 cm.

Multi-phase hepatic CT is the current standard that effectively diagnoses 63%–87% of focal changes in the liver. In many cases, standard MRI is sufficient for differentiating between benign and malignant tumors, but the results are often inconclusive. DW-MRI has emerged as a highly promising technique for oncological imaging, and it is used at various stages of oncological treatment.

The discussed method does not require the administration of intravenous contrast, therefore, it is easy to repeat and useful in patients who suffer from severe renal dysfunctions and are at the risk of nephrogenic systemic fibrosis.

In diagnosis of hepatic metastases, the sensitivity of 18F-FDG-PET/CT scans reaches up to 96%, and their specificity is estimated at 75%.

Conclusions: Among various imaging techniques diffusion-weighted imaging has emerged recently as a highly promising one.

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1. Introduction

The widespread availability of non-invasive radiological and diagnostic imaging techniques significantly contributed to the detectability of focal lesions in the liver. Accidentally detected benign tumors occur in around 15% of the healthy population,²⁴ and the probability that focal changes are malignant in persons with no cancer history does not exceed 1%.^{13,24} It is estimated that around 20% of focal liver lesions (which are not simple cysts) observed in patients with malignancies are benign, but such changes are regarded as metastases until they are ruled out. Metastatic tumors account for 95% of all hepatic malignancies, while primary tumors for only 5%.

The liver is the second most common site of metastasis after regional lymph nodes.¹⁶ In around 90% of cases, liver metastases are multifocal. The size of metastatic foci may vary, and it may exceed 10 cm. Lesions smaller than 2 mm are not detected by the available imaging methods.

Subject to the degree of vascularization, metastases are classified as richly or weakly vascularized. Richly vascularized (hypervascular) tumors are characterized by rapid, early contrast wash-in, and they are more enhanced than the remaining liver parenchyma in the arterial phase of dynamic magnetic resonance imaging (MRI) after intravenous contrast administration. Due to a higher wash-out rate, a rapid drop in signal intensity is observed in metastases in later phases of dynamic MRI (computed topography – CT), and ultimately, those lesions become hypointensive compared to a normal liver.

The more frequently encountered weakly vascularized metastases are characterized by low blood flow in the tumor, and their contrast enhancement remains low at all stages of a dynamic exam. Hypovascular metastases are most often caused by colorectal cancer, pancreatic cancer, lung cancer, pharyngeal carcinoma, melanoma, ovarian cancer, breast cancer, cervical cancer and liposarcoma. Infiltrations in non-Hodgkin lymphoma and Hodgkin lymphoma are also hypovascular.

The liver is also affected by benign tumors which are often very difficult to differentiate from malignant neoplasms. The most common benign lesions are cysts (5%–10% of the population), hemangiomas (5%–20%),^{13,24} foci of fatty degeneration and focal nodular hyperplasia (around 3%). Less frequent benign tumors include adenomas (mostly in women using hormonal contraceptives, 3–4/100,000)²⁴ and abscesses. In most cases, hepatic metastases have to be differentiated from hemangiomas owing to their similar appearance in imaging tests and the high frequency of hemangioma occurrence.

2. Aim

This article reviews the available methods for diagnosing focal liver lesions on the basis of current literature.

3. Discussion

3.1. Ultrasonography

Ultrasonography with or without contrast agents is the most common and generally the first imaging method used to

examine the parenchymal organs of the abdomen, including the liver. The diagnostic precision of a conventional ultrasound test in detecting and differentiating focal hepatic lesions is estimated at 62%.¹³ Its sensitivity for the detection of metastases ranges from 40% to 80%,^{9,13,31} subject to the tumor's diameter and the examiner's experience, and it rarely exceeds 80%. It should be noted, however, that the majority of metastatic tumors are small, and the sensitivity of ultrasound tests decreases dramatically to 20% for foci smaller than 1 cm.¹³

Intraoperative ultrasound (IOUS) imaging, which requires probes with a frequency of 7.5 MHz and higher, is characterized by improved spatial resolution, and it supports the detection of surface-located tumors with a diameter of only 2 mm.

Elastography is a new non-invasive technique that complements a basic ultrasound exam. This method has been most often applied to characterize breast tumors.⁶ It is also used to examine patients with chronic liver diseases.

3.2. Computed tomography

A CT scan of the liver without the intravenous administration of contrast media has limited diagnostic value.¹ Multi-phase hepatic CT (MDCT) is the current standard that effectively diagnoses 63%–87% of focal changes in the liver.²⁵

3.3. Magnetic resonance imaging

MRI is emerging as the most accurate method for detecting and differentiating focal liver lesions.^{16,17,30} It provides better contrast between different soft tissues than CT, and the latest MRI scanners offer spatial and temporal resolution comparable with that of CT. MRI has a small number of absolute contraindications, such as a heart pacemaker, a metallic foreign body in the eye or cochlear implants.

Conventional MRI, including T1-weighted imaging with and without contrast enhancement, T2-weighted imaging, fat suppression sequences (SPAIR – spectral attenuation with inversion recovery, STIR – short T1 inversion recovery, chemical shift imaging) and MR angiography support determinations of the size and location of hepatic tumors (including in relation to blood vessels and bile ducts) and, to a certain extent, evaluations of tumor tissue composition. In many cases, standard MRI is sufficient for differentiating between benign and malignant tumors, but the results are often inconclusive.

MRI scans performed with the use of hepatotropic contrast agents which are captured and excreted by the hepatocytes support the differentiation of tumors which contain normal hepatocytes from lesions that do not contain hepatocytes or contain abnormal hepatocytes.

Hepatotropic contrast agents improve the detectability of small (<1 cm) focal liver lesions. In patients affected by renal failure, contrast agents containing gadolinium may cause nephrogenic systemic fibrosis (NSF); therefore, kidney function has to be examined before the administration of a contrast

agent.¹¹ A multi-phase contrast CT/MR examination generally involves three phases:

- (1) early arterial phase (scan delay of 10 s) or arterial phase (delay of 15–25 s),
- (2) portal venous phase (delay of 60 s),
- (3) equilibrium phase (delay of 120 s after contrast administration or 180 s in patients with liver cirrhosis).^{17,21,24}

MRI of the liver may be complemented by MR cholangiography which images the biliary tract and the pancreatic duct without the administration of a contrast medium. Since the development of MR cholangiography, endoscopic retrograde cholangiopancreatography (ERCP) has been used as a therapeutic rather than a diagnostic procedure.²⁷

Conventional MRI techniques effectively differentiate between benign and malignant lesions only in some cases,²⁷ which is why new MRI methods offering enhanced soft-tissue visibility are researched (Table 1).

3.4. Diffusion-weighted MRI

Diffusion-weighted MRI (DW-MRI) makes use of the motion of water molecules within extracellular/extravascular space. In biological systems, diffusion is influenced by the shape and size of extracellular space, the properties of cell membranes, the content of macromolecules as well as the exchange of water between the intracellular and the extracellular compartment. The shape and the size of extracellular space are determined mainly by the size, arrangement and density of cells.^{12,14,22} DW-MRI provides information about tissue architecture and, indirectly, about the microstructure of the examined tissues.^{12,14}

Diffusion of water molecules also takes place inside the cell (where it is determined by the size and number of intracellular structures and the amount of cytoplasm), but this process has a negligible effect on MR water diffusion imaging.

Blood flow and perfusion, heart pulse and respiratory movements influence the observed motion of water molecules, and they can reduce the accuracy of water diffusion measurements.^{12,14,22} Blood flow in microcapillaries mimics diffusion, and it has the most profound effect on DW images at low values of the b -factor ($b \leq 100$ s/mm²).^{12,14}

DW-MRI is a spin-echo sequence or a gradient-echo sequence which contains an extra pair of gradients, i.e. diffusion gradients.¹⁴ Signal intensity (SI) in DW images reflects the net movement of spins and its attenuation depends on the magnitude of molecular translation and diffusion weighting. The latter is determined by the strength of the diffusion gradients, the duration of the gradients, and the time between the gradient pulses.

The parameter that summarizes the influence of the gradients on the diffusion weighted images is the b -factor (s/mm²), which is given by the following formula:

$$b = \gamma^2 G^2 \delta^2 (\Delta - \delta/3)$$

where γ is the gyromagnetic ratio, G the amplitude of the two diffusion gradient pulses, δ the duration of the pulses, Δ the time between the two pulses.

Thus, the ratio of diffusion-weighted signal to non-diffusion-weighted signal is

$$S/S_0 = \exp(-\gamma^2 G^2 \delta^2 (\Delta - \delta/3) D) = \exp(-bD)$$

where S_0 is the signal intensity without the diffusion weighting, S the diffusion-weighted signal and D the diffusion coefficient (a measure of the strength (velocity) of diffusion in tissue; the stronger the diffusion, the greater the diffusion coefficient, i.e. the apparent diffusion coefficient – APC).

In DW-MRI examinations, the lowest b -value is nearly always 0 s/mm² (less frequently 50 s/mm²), and the highest b -value is noted in the range of 750 s/mm² to 1000–1400 s/mm².^{7,12,14,20,22} The successive parts of the sequence are images acquired at $b > 0$. The data obtained from measurements of at least two diffusion acquisitions at different b -values support quantitative measurements of the mobility (diffusion) of water molecules. A measure of molecule mobility is the ADC which is expressed in mm²/s.

$$ADC = -\frac{1}{b_1 - b_0} \ln\left(\frac{S}{S_0}\right)$$

where b_1 is the value of b -factor, b_0 the value of b -factor without the use of gradients, T_2 the weighted image, S the diffusion-weighted signal, S_0 the signal intensity without the diffusion weighting.

Directional and index DW images contain elements of images dependent on diffusion and relaxation time T_2 , but in ADC maps, the T_2 shine-through effect is eliminated.^{14,26} Changes in water diffusion in tissues analyzed by DW-MRI result mainly from variations in the volume of extracellular space. A reduction in extracellular space can be caused by an increase in cell volume (as observed in, for example, cytotoxic swelling) or an increase in the number of cells or macromolecules per unit volume (as observed in, for example, tumors and abscesses). The above contributes to a phenomenon known as restricted diffusion.^{2,14,22,28}

DW-MRI does not require the administration of intravenous contrast; therefore, it is easy to repeat and useful in patients who suffer from severe renal dysfunctions and are at the risk of nephrogenic systemic fibrosis.

Malignant tumors generally restrict diffusion, and the ADC of malignancies is clearly lower than that of benign lesions.^{1,2,7,8,10,14,20} In malignant tumors, high cellular density, disorganized tissue structure and greater irregularity of extracellular space decrease the mobility of water molecules and restrict diffusion, and such tissues are characterized by high signal intensity in DW images with high b -values and low values of ADC.^{12,14,22} An absence of restricted diffusion is generally regarded as an indication of non-malignant lesions. Generally, in high b -value DW images, benign lesions are isointense in comparison with healthy organs, and they are characterized by high SI in ADC maps^{12,14,22,28} (Figs. 1 and 2, Table 2).

The accuracy of DWI is determined by various factors, mostly tumor size and the structure of tumors and organs, as well as the applied technique and patient cooperation. In organs with a specific structure, such as the spleen, tonsils or testes, the diffusion of water molecules is impaired. Differences in diffusion are too small to support correct imaging of

Table 1 – Most frequent characteristics of focal liver lesions displayed by different imaging techniques.

Focal lesion	USG	CT without contrast	MR			Dynamic examination after intravenous contrast administration			
			T1-W images	T2-W images	Change of SI in phase/contraphase	Aortic phase CT/MR	Portal phase CT/MR	Equilibrium phase CT/MR	Hepatic-cellular phase MR
Cyst	Apnea	↓	↓	↑	No	No enhancement	No enhancement	No enhancement	No enhancement
Hemangioma	↑	↓	↓	↑	No	Strong, mostly peripheral	Progressive enhancement from periphery	Progressive enhancement from periphery	Hypointensive
FNH	↕ Central scar	↕↔	↕↔	↕↔	No	Small n – homogenous Hyperdense/hyperintensive Strong (no scar)	Hyperdense/hyperintensive	Hyper/isodense Hyper/isointensive	Iso/hyperintensive (scar enhancement)
Adenoma	↕↔ Frequently non-homogenous	↕↔	↕↔	↕↔	Yes	Quite strong Hyperdense/hyperintensive	Isodense/isointensive	Isodense/isointensive	Hypo/isointensive
HCC	↓	↓	↕	↑	Yes	Quite strong Hyperdense/hyperintensive	Hypo/isodense Hypo/isointensive	Hypo/isodense Hypo/isointensive	Hypo/isointensive
Hypervascular metastasis	↕	↓	↓	↑	Yes	Strong Hyperdense/hyperintensive	Hypo/isodense, hypo/isointensive	Hypodense, hypointensive	Hypointensive
Hypovascular metastasis	↕	↓	↓	↑	No	Weak/peripheral Hyperdense, hyperintensive	Hyperdense, hyperintensive	Hypodense, hypointensive	Hypointensive

↓ – SI/density/focal lesion echogenicity lower than in a normal liver.

↑ – SI/density/focal lesion echogenicity higher than in a normal liver.

↕ – SI/density/focal lesion echogenicity similar to a normal liver.

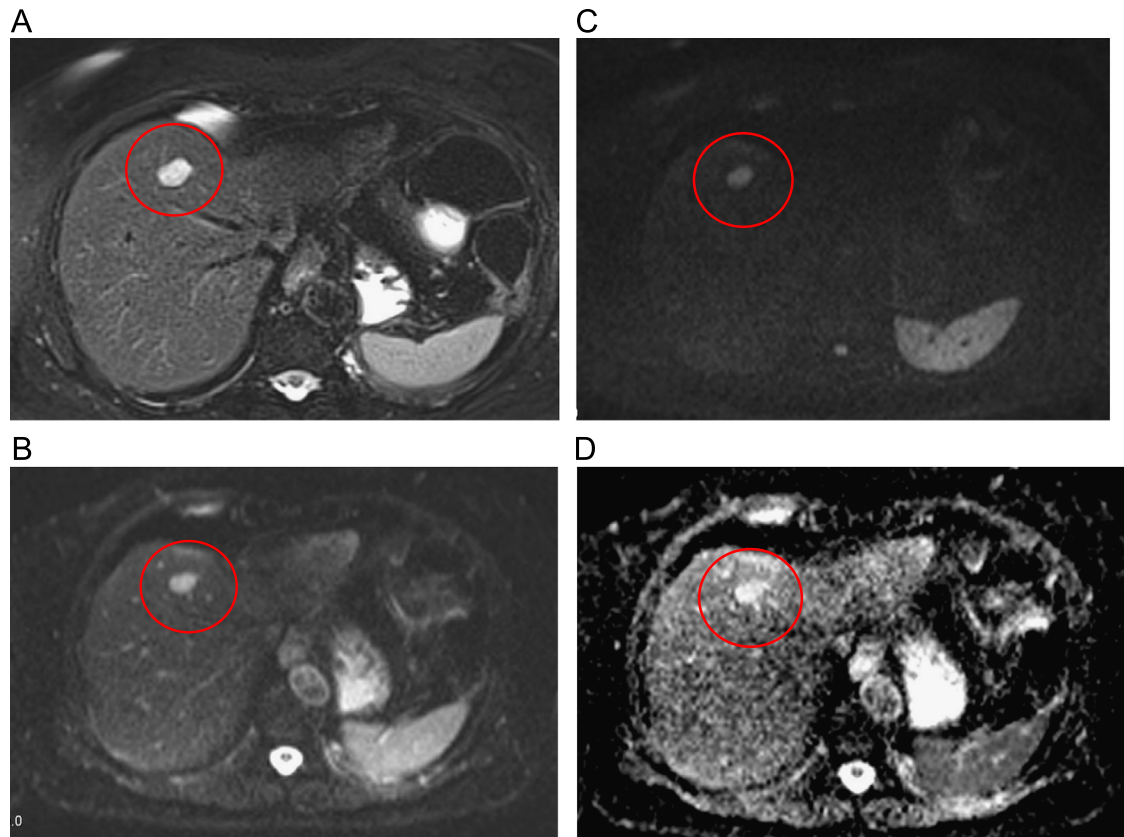


Fig. 1 – Liver hemangioma (patient, female, age: 54). DWI – no diffusion limitation (high SI in DWI b_{high} (C) + high ADC, (D) – red circle). (A) DWI $b=0$ s/mm² – high SI of hemangioma, (B) DWI $b=50$ s/mm² – high SI of hemangioma, (C) DWI $b=1000$ s/mm² – high SI of hemangioma, (D) ADC map – high ADC of hemangioma.

neoplastic infiltrations in those organs. In some organs or their parts, such as the left lobe of the liver, respiratory motion and vascular pulsation artifacts may be observed.^{12,14,22,28,29}

A b -value of 0 s/mm² delivers a T2-weighted echo-planar imaging scans image where DW images are T2-weighted images where venous vessels, similarly to the majority of focal lesions, are characterized by high SI; therefore, some small lesions (<1 cm) in the liver parenchyma may be undetected. When b -value falls in the range of 50–150 s/mm², the signal intensity of liver vessels is attenuated, and the signal intensity of most focal lesions, both benign and malignant, remains high which, with a relatively high value of SNR, supports imaging of very small lesions.^{4,14} (Table 3).

Effective cancer treatment leads to tumor cell damage, loss of cell membrane integrality and an increase in extracellular space, which generally enhances free diffusion of water molecules in neoplastic tissue and increases ADC values.^{5,14,18,23} A drop in ADC values may also be encountered in early stages of treatment, and it is attributed to cell swelling. DWI is most effective at diagnosing the early response to the treatment of breast cancer, brain tumors, primary and secondary liver cancer and bone cancer. According to Padhani, DWI differentiates between ischemic but still functioning tissues and necrotized tissues during treatment with combrestatin which damages blood vessels in tumors.²² DWI/ADC images are also used to evaluate the response to radiation therapy and the effectiveness of non-invasive treatment of liver malignancies, such as transcatheter

arterial chemoembolization (TACE) and tumor ablation (RFA, MVA, HIFU, cryoablation).^{14,18,22}

Differentiation of post-treatment lesions from neoplastic infiltrations often poses a diagnostic problem. Unrestricted diffusion practically rules out infiltration,^{14,22} and it points to post-radiotherapy swelling of tissue or an inflammatory process. Restricted diffusion, especially if accompanied by pathological contrast enhancement, is more indicative of neoplastic infiltration or a relapse.^{14,22} Post-treatment fibrosis or dehydration are characterized by low ADC values, but most misdiagnoses can be eliminated by evaluating DW images together with ADC maps. In this respect, DW-MRI appears superior to FDG PET/CT, because shortly after radiotherapy, treatment-induced inflammations often augment glucose uptake, which could produce false positive results in a PET/CT scan, but they do not restrict diffusion.^{12,14,22}

Diagnostic procedures proposed for focal lesion in the liver, uncharacteristic in ultrasonography, CT and MRI, are presented in Table 4.

3.5. Isotope imaging

The key isotope method for liver imaging is PET/CT with 18 FDG or (⁶⁸Ga)-labeled somatostatin analogs and somatostatin receptor-based scintigraphy (SPECT). In diagnoses of hepatic metastases, the sensitivity of 18F-FDG-PET/CT scans reaches up to 96%, and their specificity is estimated at 75%.³ Somatostatin receptor-based scintigraphy relies on synthetic

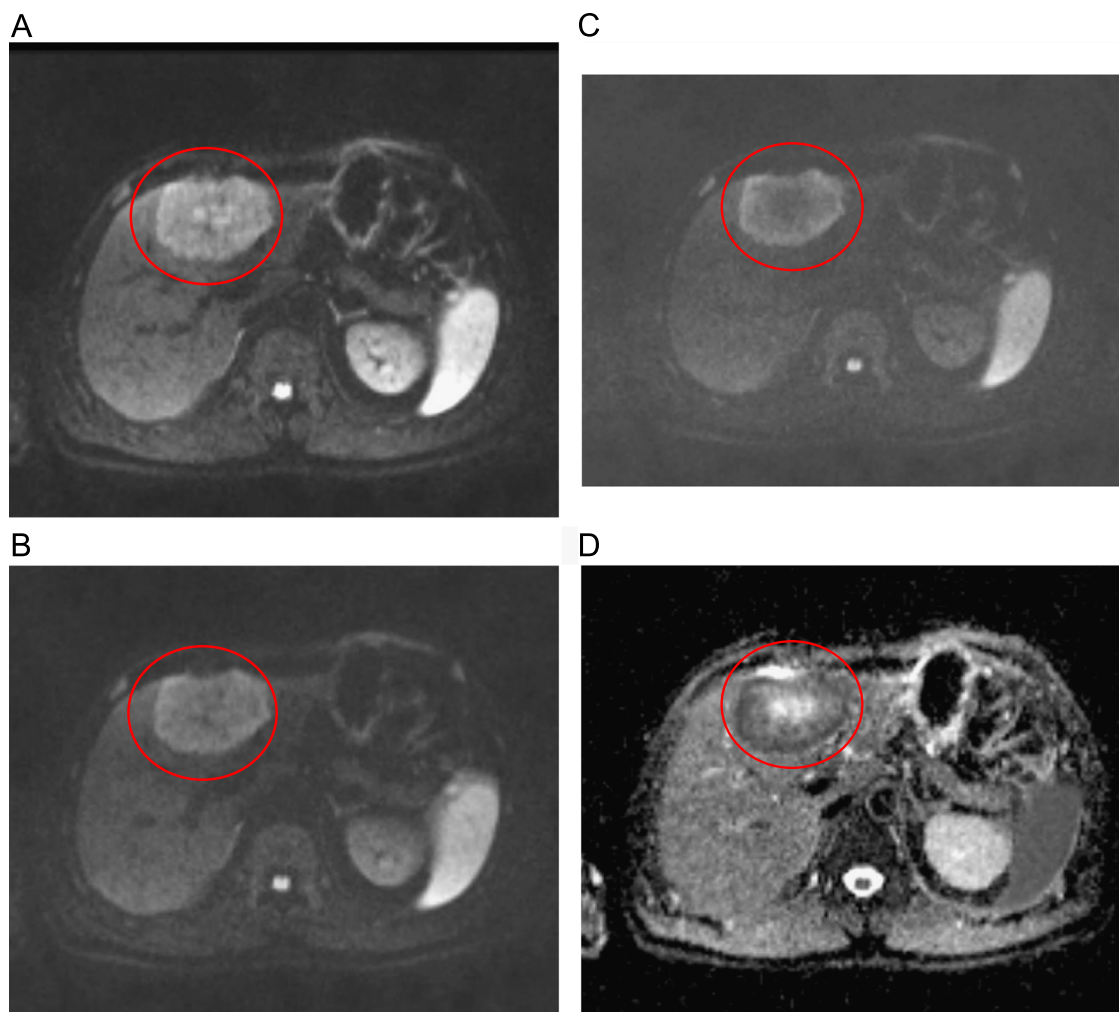


Fig. 2 – Liver metastases from colon cancer (patient, male, age: 64). DWI MR – limited diffusion (high SI in DWI b_{high} (C) + low ADC (D) – red circle). (A) DWI $b=50 \text{ s/mm}^2$ – increased SI of metastasis, (B) DWI $b=600 \text{ s/mm}^2$ – non-homogenously increased SI of metastasis, (C) DWI $b=1000 \text{ s/mm}^2$ – SI of metastasis increased on the periphery and decreased in the center, (D) ADC map – low ADC value on the periphery of metastasis – limited diffusion; high ADC value in the central part – accelerated diffusion, necrotic lesions.

Table 2 – Interpretation of DW-MR images.²²

T2-weighted image	DW image, b_{high}	ADC	Interpretation
↑↔	↑	↓	Hypercellular tumor, coagulation necrosis, abscess
↑	↑	↑	T2-shine-through effect protein-rich fluid
↑↔	↓	↓	Fibrous tissue with a small amount of water/without tumor cells
↑	↓	↑	Fluid colliquative necrosis hypocellular tumor glandular structure

Table 3 – DWI/ADC images of the most common liver focal lesions.

Focal lesion	DWI, b_{high}	ADC	Restricted diffusion
Cyst	Low SI	High	No
Hemangioma	High SI	High	No
Focal nodular hyperplasia	Low/high SI	High/low	No/yes
Adenoma	Low/high SI	High/low	No/yes
Abscess – central part – capsule	High SI	Low	Yes
	Low SI	Low	No
Metastasis	High SI	Low	Yes
Hepatocellular carcinoma (average and poorly differentiated)	High SI	Low	Yes
Hepatocellular carcinoma (well differentiated)	Moderate/low SI	Low	Yes/no

Table 4 – Diagnostic procedures propositions for focal lesion in the liver, uncharacteristic in US, CT and MRI.

Focal lesion in the liver, uncharacteristic in ultrasonography, CT and MRI	Proposed follow up/biopsy algorithm	Proposed additional examinations to obtain the diagnosis
1. Probably atypical hemangioma – Patient without known malignant disease	US follow up (possibly CT or MRI f/u): – In 3 months – In 6 months – In 12 months	– Scintigraphy with Tc marked erythrocytes Tc-99 m RBC (when lesion > 1 cm)
2. Probably atypical hemangioma – Patient with known malignant disease (main differential diagnosis with a metastasis)	CT or MRI f/u: – In 3 months – In 6 months	– Scintigraphy with Tc marked erythrocytes Tc-99 m RBC – 18 FDG PET/CT
3. Atypical solid nodule. Differential diagnosis between FNH and adenoma (high probability of a benign lesion)	CT or MRI f/u: – In 3 months – In 6 months – In 12 months – Core needles biopsy	– MRI with liver-specific contrast agent
4. Atypical solid nodule: patient without liver cirrhosis. Differential diagnosis between adenoma, HCC or metastasis (high probability of a malignant lesion)	– Core needles biopsy (if negative, then surgical biopsy) – Surgical biopsy – If biopsies negative: CT or MRI f/u in 3 months	– MRI with liver-specific contrast agent – 18 FDG PET/CT
5. Atypical solid nodule in the cirrhotic liver	– Core needles biopsy – Surgical biopsy If biopsies negative CT or MRI f/u in 3 months	– MRI with liver-specific contrast agent
6. Atypical cystic-solid nodule. Differential diagnosis between HCC, metastasis vs abscess	– Surgical biopsy	MRI+DWI

somatostatin analogs which accumulate in neuroendocrine tumors. According to numerous studies, scintigraphy with technetium-labeled red blood cells (Tc-99m RBC) has 99% specificity for the detection of hemangiomas,¹⁹ but owing to the discussed method's low spatial resolution, its specificity for tumors smaller than 2 cm is considerably lower.

4. Conclusion

Among various imaging techniques DWI has emerged recently as a highly promising one.

Conflict of interest

None declared.

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